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(54) **CONTOUR GUIDED DEFORMABLE IMAGE REGISTRATION**

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(57) **ABSTRACT**

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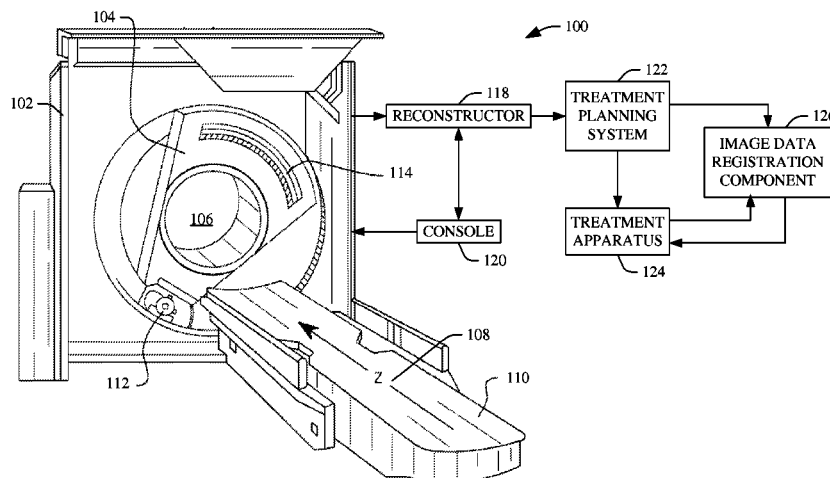
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G06K 9/3216; G06K 2209/05

A method includes obtaining first volumetric image data, which is acquired at a first time, including a region of interest with a structural feature located at a first position. The method further includes obtaining second volumetric image data, which is acquired at a second different time, including the region of interest with the structural feature located at a second different position. The method further includes determining a registration transformation that registers the first and second volumetric image data such that the at least one structural feature in the first volumetric image data aligns with the at least one structural feature in the second volumetric image data. The registration transformation is based at least on a contour guided deformation registration. The method further includes generating a signal indicative of the registration transformation.

25 Claims, 4 Drawing Sheets



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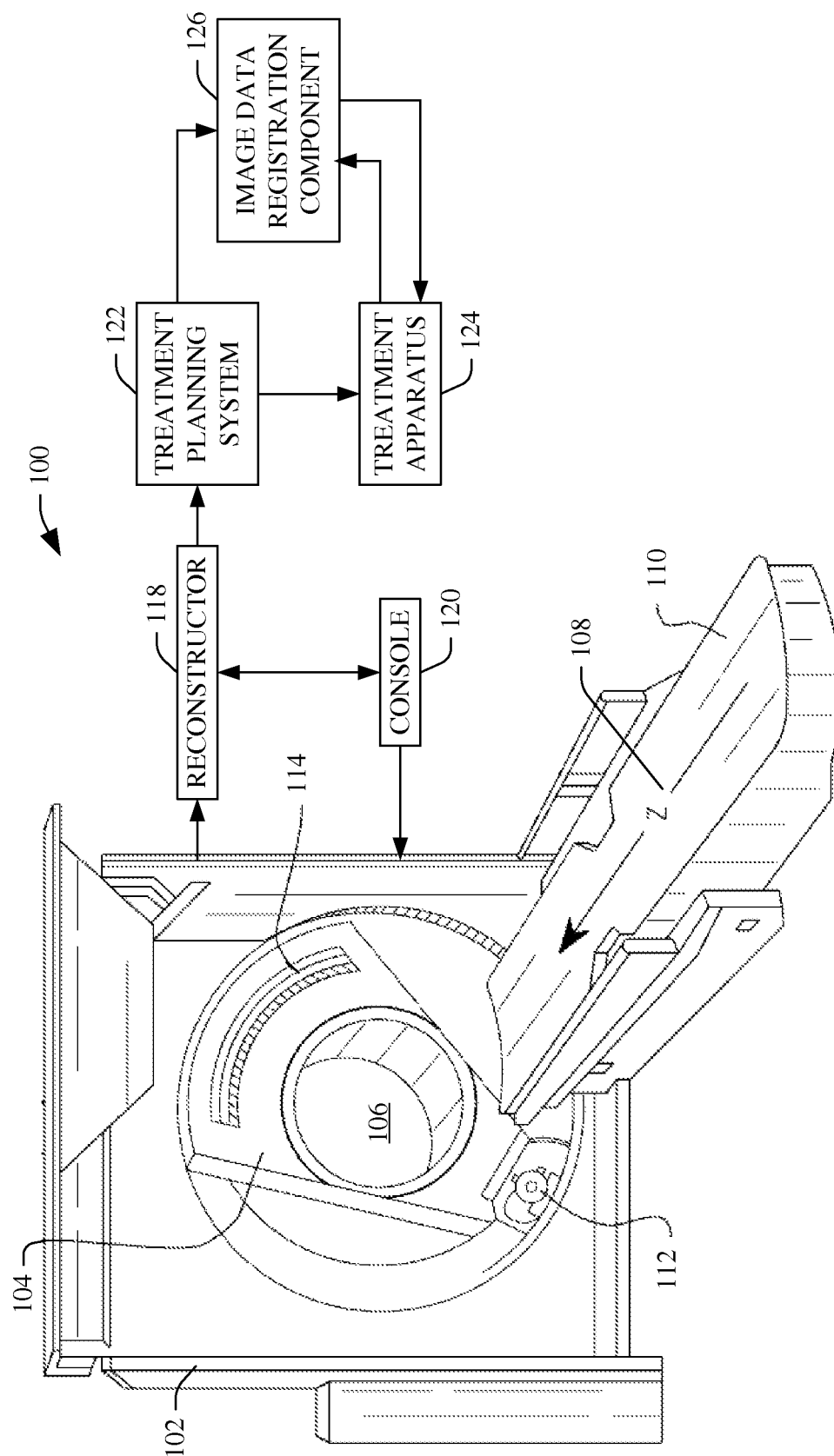


FIGURE 1

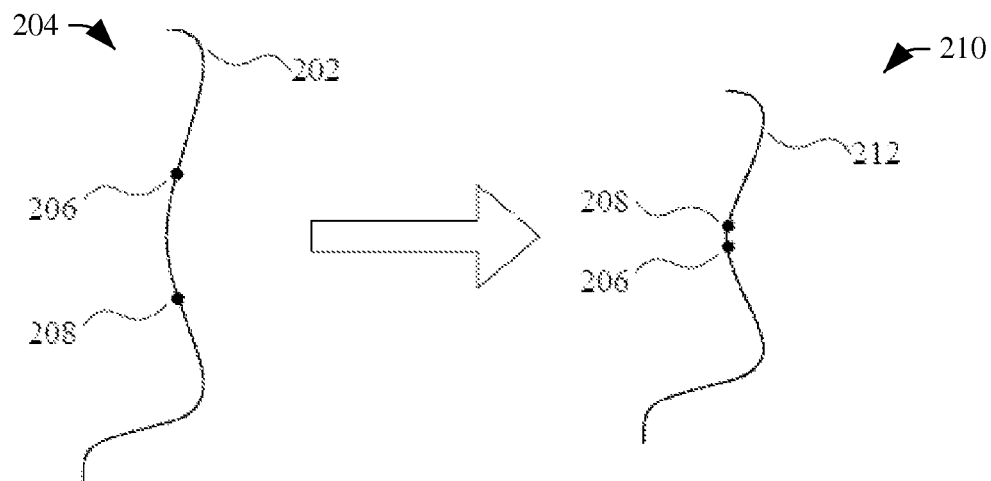


FIGURE 2



FIGURE 4

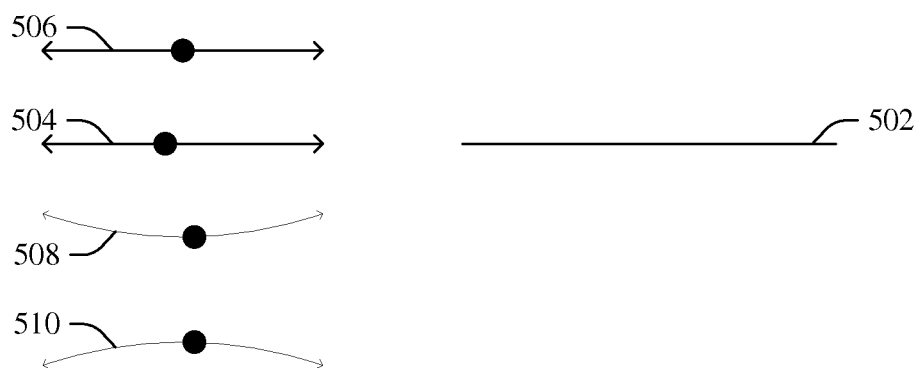


FIGURE 5

126

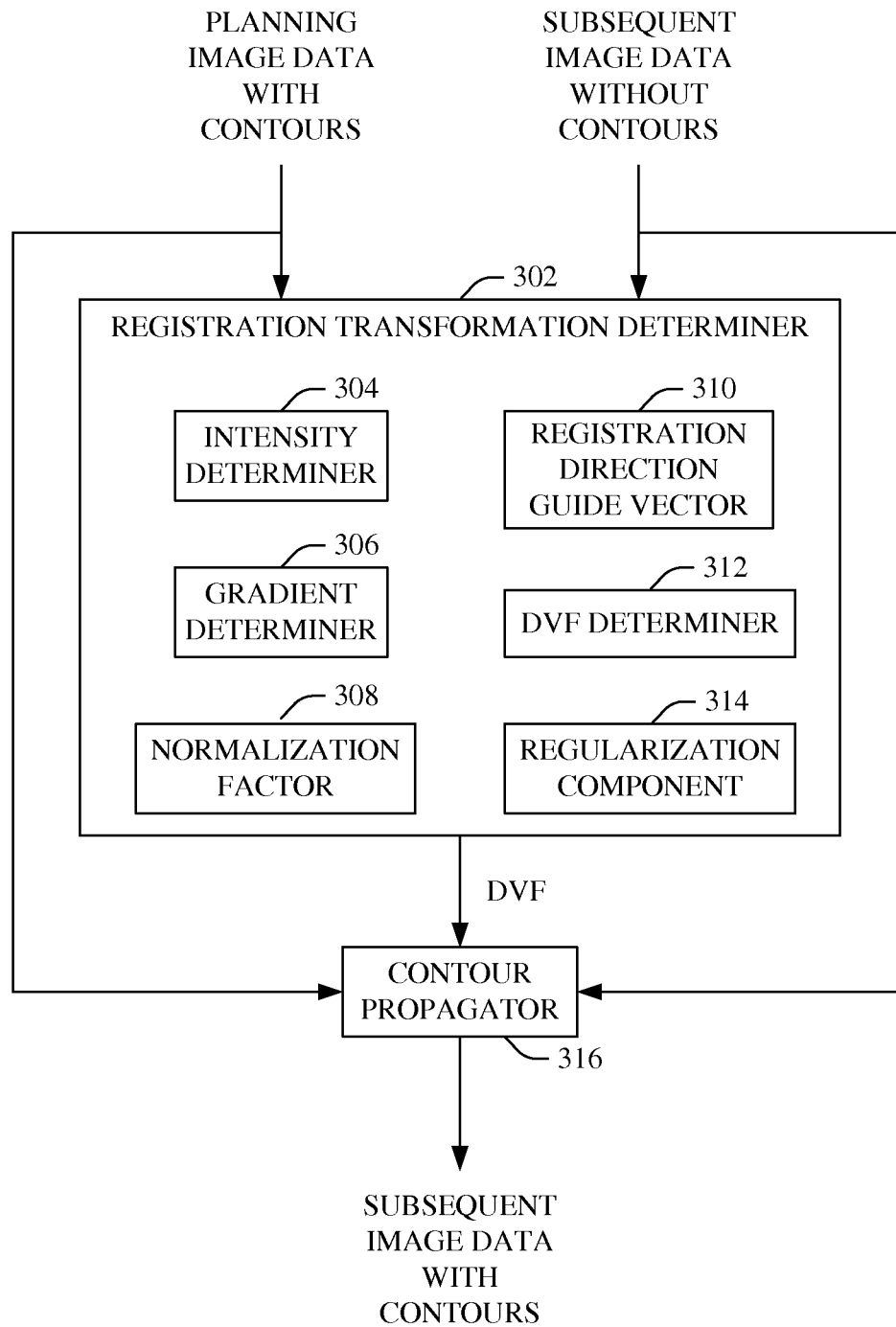


FIGURE 3

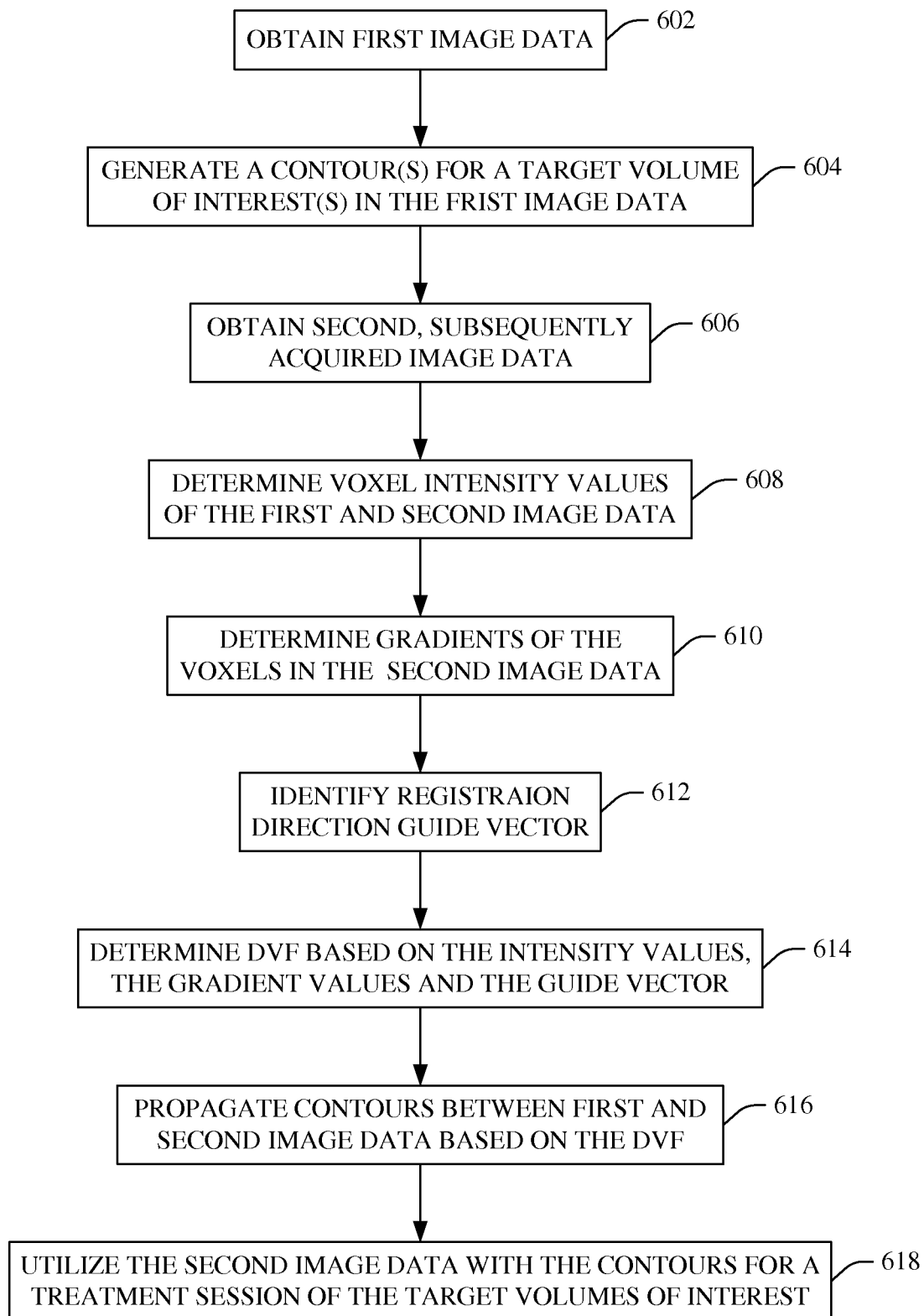


FIGURE 6

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CONTOUR GUIDED DEFORMABLE IMAGE REGISTRATION

CROSS REFERENCE TO RELATED APPLICATIONS

This application is a national filing of PCT application Serial No. PCT/IB2011/055638, filed Dec. 13, 2011, published as WO 2012/080949 A1 on Jun. 21, 2012, which claims the benefit of U.S. provisional application Ser. No. 61/423,150 filed Dec. 15, 2010, which is incorporated herein by reference.

FIELD OF THE INVENTION

The following generally relates to image processing and more particular to contour guided deformable image registration, and is described with particular application to computed tomography (CT) and radiation therapy treatment planning; however, the following is also amenable to other imaging modalities, such a magnetic resonance imaging (MRI), positron emission tomography (PET), etc., and/or applications, and to other treatment modalities such as focussed ultrasound, interferential therapy, transcutaneous electrical nerve stimulation, pulsed shortwave therapy or laser therapy.

BACKGROUND OF THE INVENTION

Radiation treatment planning is the process creating a radiotherapy treatment plan for treating a tumor(s) via ionizing radiation. For treatment planning, the subject is scanned and the resulting volumetric image data is used as initial reference or planning image data to create a treatment plan for tumors or target volumes, segmented or contoured into regions of interest (ROI) in the image data. With radiotherapy, the prescribed radiation dose is delivered in a fractionated manner, with the radiation dose being divided and given over a number of treatments, which may span several weeks. Unfortunately, daily physiological changes (e.g., organ filling, weight loss, etc) can cause the tumor volume and surrounding anatomical structures to move and change in shape during the course of the therapy such that continuing to follow the initial plan may result in an actual received dose distribution the differs from the planned dose distribution. Similar modifications are needed in any plan for directing energy at particular tissue sites for which the map may change in the course of treatment, such as interferential therapy, transcutaneous electrical nerve stimulation, pulsed shortwave therapy, or laser therapy.

As a result, the initial plan should be adapted to match the new location and shape of the target volume and surrounding anatomical structures based on subsequently acquire image data such as image data acquired during a treatment session (in-treatment). Unfortunately, the workload involved in the such adaptive re-planning can be complex and time consuming as this involves delineation or segmentation of tissue of interest and anatomical structures from latest image data for the patient. In an alternative approach, a deformable registration is used to estimate a voxel-to-voxel mapping or transformation between initial image data and latest image data. Generally, such image registration is the process of aligning features in different images by applying a transformation to one of the images so that it matches the other. The transformation is used to propagate the contours in the initial image data to contours in the latest image data.

One such registration includes the Demons deformable image registration, which is described in Thirion, J. P.,

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“Image matching as a diffusion process: an Analogy with Maxwell’s demons,” Medical Image Analysis, 1988, volume 2, number 3, pp. 243-260. Generally, Demons deformable image registration takes two images as input and produces a displacement or deformation vector field (DVF) that indicates the transformation that should be applied to voxels of one of the images so that it can be aligned with the other image. The Demons deformable image registration is an intensity (i.e., gray level) based registration in which the DVF is calculated, based on optical flow and via an iterative process, from local image information only, using a matching process that climbs the gradient of image intensity either upward or downward, in the direction of maximum steepness, in a manner that matches the gray levels as quick as possible. Unfortunately, with only the image gradient to guide the deformation process, as in the Demons deformable image registration, sideways movement of voxels is uncontrolled. The direction of maximum steepness may not be the direction in which tissue actually moved, and (since it is computed by the noisy process of estimating a gradient, composed numerically approximated derivatives) may vary unsteadily. This can lead to lack of smoothness and hence to geometric discontinuity in the deformed image and jaggedness in the propagated contours.

SUMMARY OF THE INVENTION

Aspects of the present application address the above-referenced matters and others.

According to one aspect, a method includes obtaining first volumetric image data, which is acquired at a first time, including a region of interest of a subject, wherein at least one structural feature in the region of interest is located at a first position in the first volumetric image data. The method further includes obtaining second volumetric image data, which is acquired at a second time, including the region of interest of the subject, wherein the at least one structural feature in the region of interest is located at a second position in the second volumetric image data. The second time is subsequent to the first time, and the first and second positions are different positions. The method further includes determining a registration transformation that registers the first and second volumetric image data such that the at least one structural feature in the first volumetric image data aligns with the at least one structural feature in the second volumetric image data. The registration transformation is based at least on a contour guided deformation registration. The method further includes generating a signal indicative of the registration transformation.

According to another aspect, a system includes a processor that determine a registration transformation that registers two images, wherein the registration transformation is determined based at least on voxel intensity values of the two images, voxel intensity gradient values for one of the two images, and guide vector values that indicates a direction of the registration.

According to another aspect, a method includes determining a deformation field vector which registers two images based on a contour guided deformable image registration.

BRIEF DESCRIPTION OF THE DRAWINGS

The invention may take form in various components and arrangements of components, and in various steps and arrangements of steps. The drawings are only for purposes of illustrating the preferred embodiments and are not to be construed as limiting the invention.

FIG. 1 schematically illustrates an imaging system in connection with a treatment planning system, a treatment apparatus and an image data registration component.

FIG. 2 illustrates a prior art approach to propagating contours between sets of image data.

FIG. 3 schematically illustrates an example of the image data registration component.

FIG. 4 illustrates an example approach in which contours are propagated between sets of image data across a registration direction guideline.

FIG. 5 illustrates an example approach in which contours are propagated between sets of image data along a registration direction guideline.

FIG. 6 illustrates an example method for determining a deformation field vector.

DETAILED DESCRIPTION OF EMBODIMENTS

FIG. 1 schematically illustrates an imaging system such as a computed tomography (CT) scanner 100. The scanner 100 includes a stationary gantry 102 and a rotating gantry 104, which is rotatably supported by the stationary gantry 102. The rotating gantry 104 rotates around an examination region 106 about a longitudinal or z-axis 108 one or more times for one or more data acquisition cycles. A patient support 110, such as a couch, supports a patient in the examination region 106.

A radiation source 112, such as an X-ray tube, is supported by and rotates with the rotating gantry 104 around the examination region 106. The radiation source 112 emits radiation that is collimated by a source collimator to produce a generally fan, wedge, or cone shaped radiation beam that traverses the examination region 106. A radiation sensitive detector array 114 includes a one or two dimensional array of detector pixels that respectively detect radiation that traverses the examination region 106 and generate electrical signals (e.g., a current or a voltage) indicative of the detected radiation.

A reconstructor 118 reconstructs projection data and generates volumetric image data indicative of the examination region 106. A general purpose computing system serves as an operator console 120, and includes an output device such as a display and an input device such as a keyboard, mouse, and/or the like. The console 120 includes one or more processors that execute one or more computer readable instructions encoded on computer readable storage medium and/or carried by a signal, a carrier wave or the like. In one instance, the executing instructions allow a user to control operation of the system 100.

The illustrated imaging system 100 is shown in connection with a treatment planning system 122 and a treatment apparatus 124. The treatment planning system 122 can be used to simulate treatment response to treatment and/or generate treatment plans for the treatment apparatus 124 based on the image data from the imaging system 100. Additionally or alternatively, the treatment planning system 130 can use information from other imaging modalities (e.g., MRI, PET, etc.) and/or other image data for generating one or more treatment plans.

The treatment system 130 may be configured for implementing radiation therapy (external beam, brachytherapy, etc.), chemotherapy, particle (e.g., proton) therapy, high intensity focused ultrasound (HIFU), ablation, a combination thereof and/or other treatment, such as interferential therapy, transcutaneous electrical nerve stimulation, pulsed shortwave therapy, or laser therapy. The illustrated treatment system 130 includes a radiation therapy system configured for intensity-modulated radiotherapy therapy (IMRT) and/or other radio-

therapy, and includes an on-board volumetric imaging, which can be used to generate in-treatment image data generated during a treatment session.

An image data registration component 126 is configured to generate a registration transformation (this may be stored either directly as a transformation, giving for each point the point to which it corresponds, or as a displacement or deformation vector field (DVF) giving for each point the vector from that point to the point to which it corresponds) that registers image data such as planning image data and subsequently acquired (e.g., in-treatment) image data. In the illustrated example, the image data registration component 126 uses the DVF to propagate contours, such as contours identifying target volumes of interest (e.g., tumors), in the planning image data to contours for the target volumes of interest in the subsequently acquired image. Such propagation may facilitate for compensating for target volumes of interest that have changed shape (e.g., shrunk) and/or location over time.

As described in greater detail below, the image data registration component 126 employs a gray level intensity based contour guided deformable image registration in which registration of a voxel in the planning image data with a corresponding voxel in the subsequently acquired image data is guided along or across a guide direction vector such that sideways movement (which could lead to lack of smoothness and hence to geometric discontinuity in the deformed image and jaggedness in the propagated contours) of voxels is mitigated.

FIG. 2 shows an example of such sideways movement. A contour 202 represents a contour in planning image data 204 and includes two points 206 and 208, which are deformably registered with subsequent image data 210. In this example, the two points 206 and 208 move at right angles to the contour 202 (and thus in the direction of steepest change), but these motions cross, so that after the transformation they are located on opposite sides in the propagated contour 212 in the subsequent image data 210, compared to their positions along the contour 202. As a result, some points on the contour 212 are reached by more than one point each on the contour 202. This may lead to a crumpled transformation, having geometric discontinuity and jaggedness. The contour guided deformable image registration mitigates such movement.

Returning to FIG. 1, the image data registration component 126 can be part of a computing system such as a computer, the console 120, the treatment planning system 122, and/or other system. A suitable computing system includes one or more processes that execute computer readable instructions encoded on local and/or remote computer readable storage medium. Such instructions can include all or a sub-portion of the instructions for implementing the contour propagating component 316. Additionally or alternatively, the instructions can be carried by a signal such as a carrier wave or the like.

FIG. 3 illustrates schematically illustrates an example of the image data registration component 126.

The illustrated contour propagating component 316 includes a registration transformation determiner 302, which receives planning image data with contours and subsequently acquired image data without contours.

An intensity determiner 304 determines the gray level intensity of each voxel in each of the reference and subsequent image data. In the illustrated embodiment, each voxel value corresponds to a gray level intensity values indicative of the radiodensity of the anatomical tissue represented thereby.

A gradient determiner 306 determines the gray level intensity gradient of each voxel in three dimensions (x, y and z) in the subsequent image data. Generally, the gradient indicates the directional change in the intensity in the immediate neigh-

borhood of a voxel and can be determined by convolving the image data with a filter, such as the Sobel filter or other filter, and/or through other known and/or other approaches. Gradient vectors substantially larger than the average size for the image generally correspond to boundaries, such as surfaces of anatomical structure in the image data.

A normalization factor **308** facilitates preventing overshoot. In the illustrated embodiment, the normalization factor **308** is a default value, pre-determined empirically, theoretically, or otherwise, and can be modified.

A registration direction guide vector **310** defines a (straight or curved) line across or along which the registration is performed. A suitable registration direction guide vector **310** includes a contour for a target volume of interest in the planning image data and/or a clinician provided guide line. In either case, the clinician may interact with an interactive graphical user interface (GUI) to identify and/or draw the line, modify, delete, etc. the line. Examples of suitable guide lines are described in further detail with respect to FIGS. **4** and **5**.

By way of example, a processor can present a GUI, which includes one or more images and various contouring tools. A user can use the tools to identify and/or draw the line, modify, delete, etc. the line. In response, the GUI receives an input indicative of the user defined contour, modification, deletion, etc. The resulting contour can then be used for the contour guided deformation registration. The GUI, in addition to allowing a user to create, modify and/or delete contours, allow the user to activate utilization of contours.

In FIGS. **4A** and **4B**, the registration direction guide vector **310** respectively includes reference guide lines **402** and **404** across which the registration is respectively performed along lines **406** and **408** perpendicular to the lines **402** and **404**. In FIG. **5**, the registration direction guide vector **310** provides a reference line **502** along which the registration is performed, including along a line **504** overlapping the reference line **502**, a line **506** running parallel to the reference line **502**, a line **508** being pulled towards but never reaching the reference line **502**, and/or a line **510** being pushed away from the reference line **502** but never reaching an adjacent guide line. Instead of moving purely along the (estimated) direction of maximum slope in the gray levels, a point moves in a direction which is a compromise between that direction and the direction of the reference line **502**. The closer the point is to the reference line **502**, the more strongly the compromise is biased in favor of the direction of the reference line **502**, and against the gradient direction.

Note that with such an approach points in the planning image data will map to different non-sideways overlapping points in the subsequently acquired image data, maintaining their orientation with respect to each other. This is in contrast to a non-contour guided direction approach such as the approach shown in FIG. **2** in which the points **206** and **208** in the planning image data **202** were mapped sideways about the same point **212** in the subsequent image data **210**. As such, the registration direction guide vector **310** facilitates mitigating crumpling a contour when propagating the contour from planning image data to subsequently acquired image data.

Returning to FIG. **3**, a DVF determiner **312** determines a DVF based on at least one or more of the intensities determined by the intensity determiner **304**, the gradient determined by the gradient determiner **306**, the normalization factor **308** and the guide direction vector **310**. By way of non-limiting example, in one instance, the DVF determiner **312** determines a DVF ($\vec{d}(x)$) based on EQUATION 1:

$$\vec{d}(x) = \frac{[I_s(x) - I_p(x)] \nabla I_s(x)}{\|\nabla I_s(x)\|^2 + [I_s(x) - I_p(x)]^2 / K} + \frac{[I_s(x) - I_p(x)] [\nabla I_s(x) \cdot \vec{n}]}{\|\nabla I_s(x)\|^2 + [I_s(x) - I_p(x)]^2 / K} \vec{n} \quad \text{EQUATION 1}$$

wherein $I_p(x)$ represents the intensity value of the voxels of the planning image data, $I_s(x)$ represents the intensity value of the voxels of the subsequently acquired image data, $I_s(x) - I_p(x)$ represents the difference in intensity value, $\nabla I_s(x)$ represents the intensity gradient, $\|\nabla I_s(x)\|^2$ represents the size of the gradient, K represents the normalization factor, and \vec{n} represents the guide direction vector **310**.

In EQUATION 1, a first term

$$\frac{[I_s(x) - I_p(x)] \nabla I_s(x)}{\|\nabla I_s(x)\|^2 + [I_s(x) - I_p(x)]^2 / K}$$

climbs the gradient of image intensity either upward or downward without regard to any particular direction. However, in EQUATION 1, a second term

$$\frac{[I_s(x) - I_p(x)] [\nabla I_s(x) \cdot \vec{n}]}{\|\nabla I_s(x)\|^2 + [I_s(x) - I_p(x)]^2 / K} \vec{n}$$

climbs the gradient, but is constrained to move only along the direction (\vec{n}) indicated by the guide direction vector **310**.

A regularization component **314** regularizes the DVF. In this illustrated embodiment, the regularization component **314** regularizes the DVF by applying Gaussian filtering. However, other known and other regularization approaches are also contemplated herein.

The illustrated contour propagating component **316** further includes a contour propagator **316**, which propagates the contours in the planning image to the subsequently acquired image data, such that the contours continue to identify the target volumes of interest.

In the above non-limiting example, the registration transformation determiner **302** determines a DVF which is used to propagate contours of target volumes and/or anatomical structures of interest from planning to subsequently acquired image data in connection with radiation therapy. However, it is to be understood that the registration transformation determiner **302**, additionally or alternatively, can be used to determine DVFs for other applications, including non-radiation therapy application, and in particular any therapy which follows a plan directing material or energy to specific regions of tissue. In general, the registration transformation determiner **302** can be used in connection with any application in which images are registered.

FIG. **6** illustrates an example method for determining a DVF, and is described in connection with a non-limiting example in which a contour of a target volume of interest in radiation therapy planning image data is propagated to subsequently acquired image data.

It is to be appreciated that the ordering of the acts in the methods described herein is not limiting. As such, other

orderings are contemplated herein. In addition, one or more acts may be omitted and/or one or more additional acts may be included.

At **602**, first image data for a patient is obtained. The may include scanning the patient and/or obtaining image data from a previous scan of the patient.

At **604**, generate at least one contour for at least one target volume of interest in the image data.

At **606**, second image data for the patient, acquired subsequent to the first image data, is obtained. The subsequently acquired image data may correspond to image data acquired during a treatment session, image data acquired a predetermined time after the treatment session, image data acquired a predetermined time after the creation of the planning image data, etc.

At **608**, voxels intensity (gray level) values of the voxels of the first and second image data are determined.

At **610**, voxel intensity gradients are determined for the voxels in the second image data.

At **612**, a registration direction guide vector (e.g., the guide **310**) is identified. As described herein, the guide can be a contour of a target volume of interest in the planning image data and/or a clinician drawn guide line, which guides the registration either perpendicular to the guide line or parallel to the guide line.

At **614**, a deformation field vector (DVF) that registers the first and second image data, based at least on the voxels intensities, the image gradient, and the registration direction guide vector is determined.

At **616**, the DVF is used to propagate contours for target volumes and/or anatomical structures of interest in the first image data to contours for the target volumes of interest in the second image data. As described herein, such contours may identify tumors to be treated.

At **618**, a treatment session is performed based on the second image data, utilizing the contours propagated thereto.

The above may be implemented by way of computer readable instructions, which when executed by a computer processor(s), cause the processor(s) to carry out the described acts. In such a case, the instructions are stored in a computer readable storage medium associated with or otherwise accessible to the relevant computer.

The invention has been described herein with reference to the various embodiments. Modifications and alterations may occur to others upon reading the description herein. It is intended that the invention be construed as including all such modifications and alterations insofar as they come within the scope of the appended claims or the equivalents thereof.

What is claimed is:

1. A method, comprising:

obtaining first volumetric image data, which is acquired at a first time, including a region of interest of a subject, wherein at least one structural feature in the region of interest is located at a first position in the first volumetric image data;

creating a contour for the at least one structural feature on the first volumetric image data, wherein the contour identifies the at least one structural feature;

obtaining second volumetric image data, which is acquired at a second time, including the region of interest of the subject, wherein the at least one structural feature in the region of interest is located at a second position in the second volumetric image data,

wherein the second time is subsequent to the first time, and the first and second positions are different positions;

adding a direction guideline to the first volumetric image data adjacent to the contour;

determining a registration transformation that registers the first and second volumetric image data such that the at least one structural feature in the first volumetric image data aligns with the at least one structural feature in the second volumetric image data, wherein the registration transformation propagates the contour from the first volumetric image data to the second volumetric image data based on a combination of an estimated direction of a maximum slope of the contour in gray levels and the direction guideline; and

generating a signal indicative of the registration transformation.

2. The method of claim **1**, wherein determining the registration transformation includes determining a deformation field vector that extends along the direction guideline.

3. The method of claim **1**, wherein determining the registration transformation includes determining a deformation field vector that extends along a line parallel to the direction guideline.

4. The method of claim **3**, wherein the deformation field vector is pulled towards the direction guideline.

5. The method of claim **1**, wherein determining the registration transformation includes determining a deformation field vector that extends perpendicularly from the direction guideline.

6. The method of claim **2**, wherein the direction guideline is a curved line.

7. The method of claim **2**, wherein direction guideline line is a straight line.

8. The method of claim **2**, wherein the direction guideline is a user drawn line superimposed over the first image data.

9. The method of claim **1**, wherein the combination weights the direction guideline for propagating a point on the contour to the second volumetric image data as a function of a distance between the point and the direction guideline.

10. The method of claim **9**, further comprising: applying a first weight to propagate a first point on the contour based on a first distance between the point and the direction guideline, and applying a second weight to propagate a second point on the contour based on a second distance between the point and the direction guideline, wherein the first distance is less than the second distance, and the first weight is greater than the second weight.

11. The method of claim **2**, wherein the first and second volumetric image data include voxels represents gray level intensity values, and determining the registration transformation, comprising:

determining a difference in intensity value between corresponding voxels in the first and second volumetric image data;

determining an intensity gradient vector for the voxel in the second volumetric image data;

determining a normal vector that is perpendicular to the direction guideline;

determining a dot product of the intensity gradient vector and the normal vector;

determining a square of a magnitude of the intensity gradient vector;

determining a square of the difference; and

calculating a deformation field vector as the product of the difference, the dot product and the normal vector divided by a product of the square of the magnitude and the square of the difference, wherein the deformation field vector is the registration transformation.

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12. The method claim 11, further comprising:
regularizing the deformation field vector; and
normalizing the square of the difference a normalization
factor prior to calculating the deformation field vector
and using the normalized square of the difference to
calculate the deformation field vector.

13. The method of claim 1, further comprising:
presenting an interactive graphical user interface which
includes contouring tools, wherein the interactive
graphical user interface receives an input indicative of a
user defined direction guideline, wherein the user-defined
direction guideline is the generated direction
guideline.

14. A system, comprising:
a processor that determines a registration transformation
that registers two images, wherein the registration transformation
is determined based at least on voxel intensity
values of the two images, voxel intensity gradient values
for one of the two images, and guide vector values that
indicate a direction of the registration and that correspond
to a line placed that is separate from the images
and that is placed next to a contour of a structure of
interest in one of the two images, and wherein the registration
transformation propagates the contour to a second
of the two images based on a combination of an
estimated direction of a maximum slope of the contour
in gray levels and the line.

15. The system of claim 14, wherein the guide vector
values define on the line across which the registration is
performed.

16. The system of claim 14, wherein the guide vector
values define on the line along which the registration is performed.

17. The system of claim 14, wherein the line is separate and
distinct from the contour.

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18. A method, comprising:
determining a deformation field vector which registers two
images based on a contour guided deformable image
registration; and

registering the two images using the deformation field
vector, wherein the registering propagates a contour of a
structure of interest in a first image of the two images to
a second image of the two images using a weighted
registration which applies a first weight to an estimated
direction of a maximum slope of the contour in gray
levels and applies a second weight to a direction guideline
placed adjacent to the contour.

19. The method of claim 18, wherein the first image is
acquired at a first time and includes the structure of interest at
a first location and the contour, which identifies the structure
of interest, and the second image is acquired at a second
different time and includes the structure of interest at a second
different location.

20. The method of claim 19, wherein the contour is created
by a user via a graphical user interface.

21. The method of claim 18, wherein the first image is a
treatment planning image and the second image is a follow-up
image.

22. The method of claim 21, wherein the second image is
acquired during a treatment procedure.

23. The method of claim 22, wherein the treatment procedure
includes at least one of radiation therapy, chemotherapy,
particle therapy, high intensity focused ultrasound, ablation,
interferential therapy, transcutaneous electrical nerve stimulation,
pulsed shortwave therapy, laser therapy, or a combination
thereof.

24. The method of claim 18, wherein the direction guideline
is superimposed over the first image and extends along or
across the direction guideline.

25. The method of claim 18, wherein the direction guideline
is a user drawn line superimposed over the first image.

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